

The Relationship Between Ideal Lumbar Pedicle Screw Position and Superior Facet in Adolescent Idiopathic Scoliosis

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ABSTRACT

Objective: The purpose of this study was to investigate the angular relationship between the anatomic inclination of the superior facet and the desired safe straight-forward (SF) transpedicular screw trajectory in the surgical treatment of patients with adolescent idiopathic scoliosis (AIS).

Methods: The study was conducted as a retrospective evaluation. One hundred and ten lumbar vertebrae were analyzed from the preoperative computed tomography scans of 22 patients with AIS scheduled for surgery. Each lumbar vertebral segment was prepared using reformat images obtained with three-dimensional (3D) volume-rendered images. The axial angles between the relative trajectory of the implant, which was planned to be placed according to the ideal SF transpedicular pedicle screw technique, and the inclination of the superior facet joint were measured.

Results: Two hundred and twenty pedicle-facet angles of 110 vertebrae were measured on image slices showing 3D volume rendering of pedicle and facet joint together. The ideal SF orientation angle at each vertebral level was more laterally oriented than the facet tilt. Fifteen (68%) of the patients had Lenke type 1 and 7 (32%) had Lenke type 5. When the patients were divided into two groups according to Lenke type (type 1 and 5), there was no statistically significant difference in terms of the angular values of the lumbar spine ($p>0.05$).

Conclusion: When implanting a transpedicular screw to correct a scoliotic deformity, a trajectory that is no more medially inclined than the inclination of the facet joint will reduce adverse events such as medial breaching. This information can be used as supporting information when placing pedicle screws in addition to other anatomical landmarks.

Keywords: Pedicle screw, facet joint, medial breaching

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INTRODUCTION

Adolescent idiopathic scoliosis (AIS) is a three-dimensional (3D) deformity with coronal, sagittal, and axial components (1). The current gold standard treatment method in the surgical treatment of AIS is instrumented fusion of the posterior segments with transpedicular screws (2). The incidence of misplacement of pedicle screws in the lumbar spine is reported to be 5% to 41% (3). To avoid complications in scoliosis surgery, it is crucial to avoid misplacement of transpedicular screws (4). The screws should be firmly seated in the medullary canal of the bony pedicle to also provide adequate correction of the rotational deformity (5).

Multiplanar images can be thickened into slabs according to the anatomical area of interest using projection techniques such as volume rendering. Volume rendering is a technique that combines 3D perspective with versatile and interactive rendering of the entire volume of reconstructed data (6). Radiological images obtained by volume rendering are closest to the image that the surgeon sees with the naked eye in the surgical field (7).

The purpose of the present study was to investigate the relationship between the anatomic inclination of the superior facet and the desired safe transpedicular screw trajectory in the surgical treatment of AIS. To this end, the angular relationship between the superior facet joint and the pedicle screw trajectory was evaluated using postoperative computed tomography scans and volume rendering projection techniques to obtain a reliable orientation angle in the axial plane.

METHODS

Two hundred and twenty pedicle facet regions of lumbar vertebral segments from 22 patients with AIS surgically treated in our department of orthopedics and traumatology between July 2020 and March 2022 were included in the evaluation based on preoperative tomography images. Demographic data (age, sex, Lenke subtypes) were recorded. Surgical treatment of AIS was accepted as an inclusion criterion, and patients with a

diagnosis of known etiology or those with inadequate or poor imaging for measurements were excluded from the study. It was confirmed that no intracanal pathology was present on magnetic imaging studies. The study protocol was approved by the Ethics Committee of Başakşehir Çam and Sakura City Hospital (decision no: 2022.04.102). Informed consent was not needed given the nature of the study.

Radiological Evaluation

Each of the 3D lumbar vertebral images created using the volume rendering technique was sliced using the scalpel function of the program [RadiAnt DICOM Viewer (Software). Version 2021.1. Jun 27, 2021]. In this way, a bird's-eye view of the tip of the superior facet joint and the pedicle of each vertebra was obtained on the same screenshot. The screenshot was then opened in the Surgimap® measurement system (Nemaris Inc. USA) (<https://www.surgimap.com/>). For the lumbar vertebrae from L1 to L5, it was marked on the tomography that the junction of the middle and lateral thirds of the intersection of the midline of the transverse process and the corresponding superior articular process was the entry point of the pedicle screw. The trajectory of the pedicle screw was determined by combining this point with the most central point of the pedicle. The angle between the superior articular facet and the trajectory of the ideal screw passing through the pedicle was determined using the straight-forward (SF) technique (Figure 1, 2) (8). This measurement was performed for both the right and left sides. Radiographic measurements (measurements in the Surgimap app) were measured again 3 weeks later by the same observer.

Statistical Analysis

Data analysis was performed using the SPSS 24.0 program. For the descriptive characteristics, analyzes of number, percentage, mean, and standard deviation were performed. While the Mann-Whitney U test was used for paired groups, Kruskal-Wallis analyzes were performed for more than two groups. Spearman correlation test was performed for relational analysis. $P < 0.05$ was considered significant.

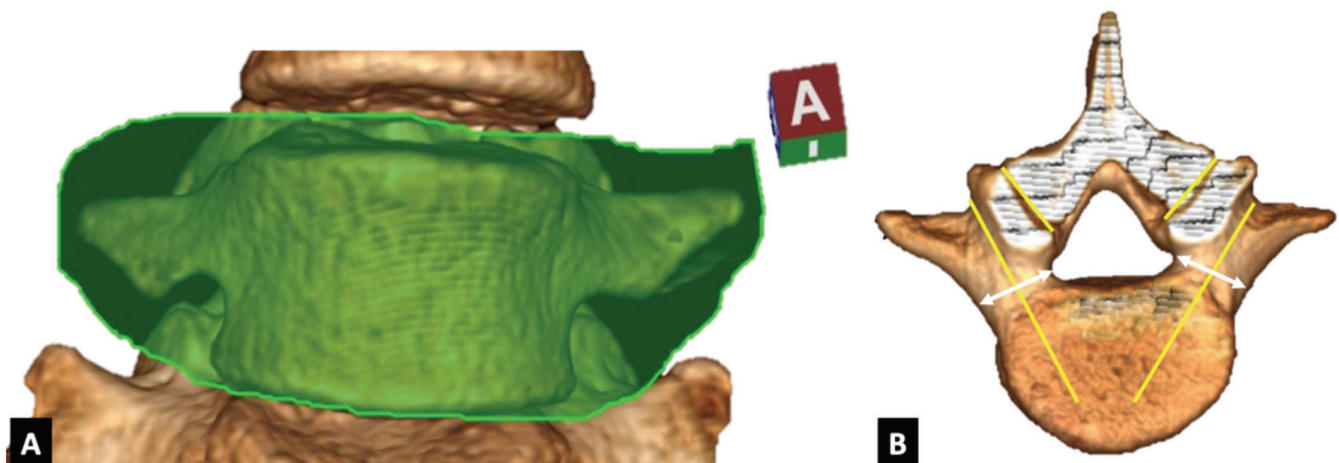


Figure 1. Cutting a three-dimensional volume-rendering image with the scalpel feature at the L5 vertebral level (A). Identification of the planned ideal transpedicular pedicle trajectory and the superior facet inclination with the top view of the obtained single vertebral level (B)

RESULTS

The mean age of the 22 patients included in the study was 14.5 ± 1.33 and two of them were male. In 3 of the patients, L5-S1 transitional vertebrae were observed as an additional anatomical variation. The angles between the axial superior facet inclination and the targeted SF pedicle trajectory of the measured vertebrae are shown in Table 1.

According to the values for skewness and kurtosis, except for the left L5 lumbar vertebra, a normal distribution was found for the angular measurements of all segments, as indicated in the

methodology, since they were all in the nominal range (-1.5)-(+1.5), parametric tests were used for the statistical analyzes. The consistency of the correlation coefficient between two separate calculation time intervals was above 0.8, indicating good agreement. According to Lenke classification, 68% of patients belonged to type 1 and 32% to type 5, and 32% had the level of lumbar apex at L2 (Table 2).

Considering the distributions of mean and standard deviation of angle measurements, the highest angles were observed at the L5 Right (18.47 ± 8.62) and L5 Left (18.4 ± 10.34) spine levels (Table 3).

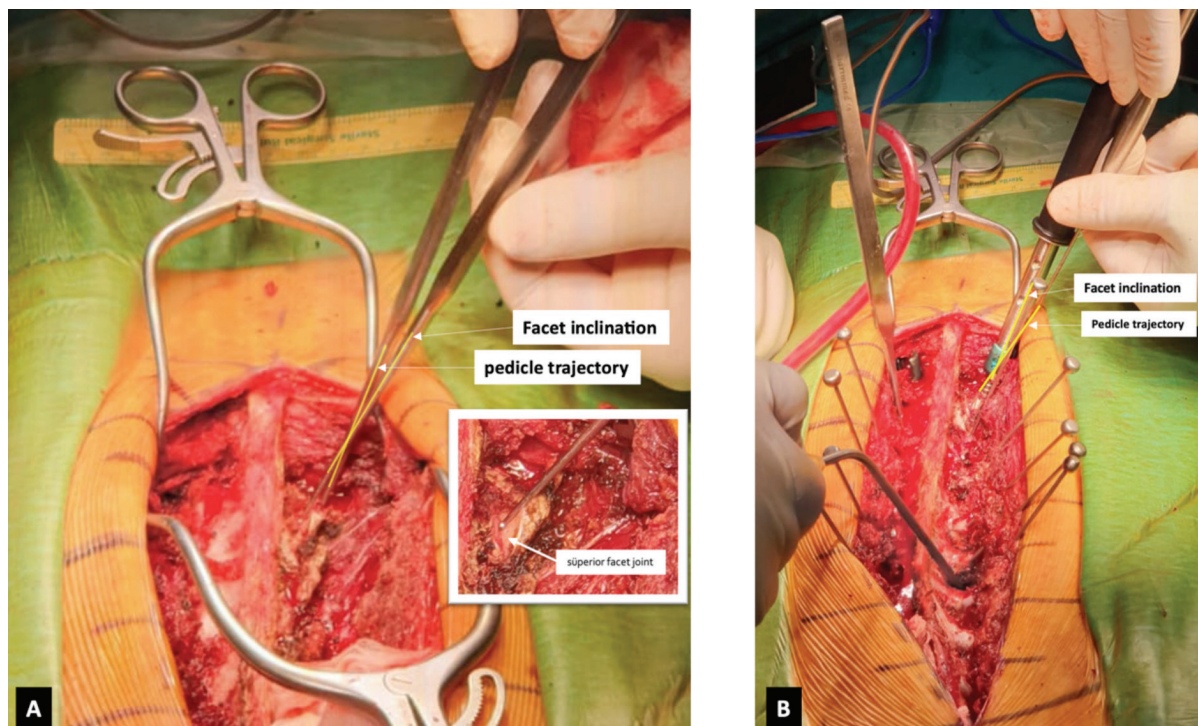


Figure 2. In one of the patients included in the study, the angle between the pedicle and the inclination of the superior facet joint is observed during surgery. Angle between two pedicle guides in A. In B, the relationship to the facet joint during pedicle screw application is seen. Note how the imaginary lines drawn in yellow cross each other. The axis of the ideal pedicle screw is more laterally directed to the inclination of the facet joint and does not go further medially than the inclination of the facet joint

Table 1. Bilateral facet-SF pedicle trajectory angular measurements for each lumbar vertebral level

Level	Mean	Minimum	Maximum	SD	Skewness	Kurtosis
L5 right	16.5	10	45.7	10.3	0.92	1.86
L5 left	15.9	12	42.6	8.9	1.2	2.92
L4 right	11.4	2.3	21.1	5.4	0.19	-0.64
L4 left	11.4	10	25.3	6.6	0.43	-0.18
L3 right	8.5	0.3	19.9	5.6	0.28	-1.03
L3 left	8.1	0.2	19.5	5.3	0.28	-0.86
L2 right	9.1	0.4	18.5	4.8	0.13	-0.34
L2 left	7.7	0.5	15.5	5.0	0.08	-1.2
L1 right	10.8	0.6	23.7	5.0	0.17	1.4
L1 left	10.4	0.5	24.8	5.4	0.45	1.3

SD: standard deviation, SF: straight-forward, L: lumbar vertebra

No statistically significant difference was found between the age groups of the patients and the mean value of the angle measurement ($p>0.05$) (Table 4).

No statistically significant difference was found between the sex and mean angular measurements of the patients ($p>0.05$) (Table 5).

Of the patients, 15 (68%) had Lenke type 1 and seven (32%) had Lenke type 5. No statistically significant difference was found when patients' Lenke types were compared with the mean of the angle measurement ($p>0.05$) (Table 6).

The lumbar modifier type was type A in 4 of the patients and type C in the remaining 18 patients. The lumbar apex was at the L1 level in 5 (23%) of 22 patients, at the L2 level in 7 (32%), at the L3 level in 6 (27%), and at the L4 level in 4 (18%) patients. No statistically significant difference was found when comparing the Lenke Lumbar Modifiers and the patients' mean angle measurements ($p>0.05$) (Table 7).

No statistically significant difference was found when comparing measurements of Lumbar Apex and mean angle ($p>0.05$) (Table 8).

According to the Spearman correlation test, a positive and statistically significant relationship was found in the relational analyzes of the following angle measurements: Between L1 L and L1 R (strong relationship), L2 L (moderate), L2 R (moderate), and L3 R (moderate); between L1 R and L2 L (moderate), L2 R (moderate), and L3 R (moderate); between L2 L and L2 R (strong), L5 L (moderate), L5 R (moderate), between L2 R and L5 R

(moderate); between L3 L and L3 R (strong), L4 L (moderate), L4 R (moderate), L5 L (moderate), and L5 R (moderate); between L3 R and L4 L (moderate), L4 R (moderate), L5 L (moderate), and L5 R (moderate); between L4 L and L4 R (strong), L5 L (strong), and L5 R (strong); between L4 R and L5 L (moderate), L5 R; and finally between L5 L and L5 R (strong) ($p<0.05$) (Table 9).

It was found that the angles measured at each lumbar vertebral level varied within a wide scale, regardless of the patients' demographic characteristics and Lenke type classification ($p<0.05$), even at the same vertebral level in different patients. In all patients, the right and left angle measurements for each vertebra were found to be similar and did not show statistical significance ($p>0.05$). Statistically significant differences were observed in the angle measurements between the same vertebral levels in different patients ($p<0.05$).

In all patients, the calculated angle between the facet inclination and the imaginary trajectory of the pedicle screw had a positive numerical value, meaning that the trajectory of the pedicle was more laterally directed than the inclination of the facet cartilage (100%).

DISCUSSION

The current study reports that osteotomy of the inferior facet before pedicle screw placement helps surgeons avoid injury to nerve tissue in the canal and prevent possible medial breaching by guiding the pedicle screw at a lower inclination (more lateral) than the axial inclination of the exposed superior facet cartilage.

The open surgical technique for AIS uses a midline skin incision and subperiosteal dissection to expose the spinous processes, laminae, facet joints, and transverse processes. Inferior facet osteotomies are performed before or after screw placement in the fusion area to help identify pedicle screw entry points, promote arthrodesis, and allow easier correction of the deformity except at the superior and inferior levels (1,9). Mattei et al. (9) recommended partial facetectomy of the inferolateral third of the inferior articular process of the upper spine. With this osteotomy, the boundaries of the facet joints can be clearly determined, and the entry point for the pedicle screw can be properly designed by removing the hypertrophic and misleading tissue; it can be ensured that the screw head can sit on a smooth surface. The current study shows that it is probably a dangerous idea to guide a transpedicular screw trajectory more medially than the inclination of the superior facet joint in the axial plane. This information may be a valuable contribution to the literature.

Amaral et al. (10) studied the safe angle with the facets that could prevent facet joint violation during screw insertion regardless of the screw insertion technique in degenerative spines. The authors analyzed imaging of patients operated for degenerative lumbar spine pathologies and defined the angle between pedicle screw and facet joint inclination as Δ -angle. Accordingly, the rate of facet injury in patients with a Δ -angle of

Table 2. Lenke type and lumbar apex distributions

	n (22)	%
Lenke type		
1	15	68.2
5	7	31.8
Lumbar apex		
L1	5	22.7
L2	7	31.8
L3	6	27.3
L4	4	18.2

L: lumbar vertebra

Table 3. Distribution of mean and standard deviation values of angle measurements

Facet-screw angle	Mean + SD		Mean $\pm$ SD
L1 R	11.1 $\pm$ 4.61	L1 L	10.78 $\pm$ 5.05
L2 R	9.62 $\pm$ 4.46	L2 L	8.82 $\pm$ 3.95
L3 R	9.75 $\pm$ 5.15	L3 L	9.41 $\pm$ 5.07
L4 R	12.43 $\pm$ 5.6	L4 L	12.46 $\pm$ 5.84
L5 R	18.47 $\pm$ 8.62	L5 L	18.4 $\pm$ 10.34

R: the angle between the superior articular facet and the trajectory line of the ideal screw at the right side, L: same angle measurement for the left side, SD: standard deviation

Table 4. Comparisons of age groups and mean angle measurements

	Age group	n (22)	Mean $\pm$ SD	U	p
L5 R	<15	10	15.93 $\pm$ 6.97	42	0.235
	≥ 15	12	20.6 $\pm$ 9.56		
L5 L	<15	10	18.35 $\pm$ 12.72	48.5	0.448
	≥ 15	12	18.43 $\pm$ 8.46		
L4 R	<15	10	11.02 $\pm$ 6.15	46.5	0.373
	≥ 15	12	13.61 $\pm$ 5.07		
L4 L	<15	10	11.7 $\pm$ 6.65	52	0.598
	≥ 15	12	13.1 $\pm$ 5.27		
L3 R	<15	10	9.19 $\pm$ 4.9	53.5	0.668
	≥ 15	12	10.21 $\pm$ 5.51		
L3 L	<15	10	9.17 $\pm$ 5.72	56.5	0.817
	≥ 15	12	9.6 $\pm$ 4.72		
L2 R	<15	10	8.64 $\pm$ 2.95	48	0.429
	≥ 15	12	10.44 $\pm$ 5.41		
L2 L	<15	10	8.1 $\pm$ 3.08	50.5	0.531
	≥ 15	12	9.42 $\pm$ 4.6		
L1 R	<15	10	10.9 $\pm$ 4.42	59	0.947
	≥ 15	12	11.25 $\pm$ 4.96		
L1 L	<15	10	11.56 $\pm$ 4.03	45	0.323
	≥ 15	12	10.13 $\pm$ 5.86		

SD: standard deviation, U: The Mann-Whitney U value, L: lumbar vertebra, R: right

Table 5. Comparisons of gender and mean angle measurements

	Gender	n	Mean $\pm$ SD	U	p
L5 R	Female	18	19.1 $\pm$ 9.37	29	0.551
	Male	4	15.65 $\pm$ 3.2		
L5 L	Female	18	19.33 $\pm$ 11.2	26	0.394
	Male	4	14.15 $\pm$ 2.85		
L4 R	Female	18	11.97 $\pm$ 5.58	26	0.394
	Male	4	14.52 $\pm$ 6.04		
L4 L	Female	18	12.13 $\pm$ 5.53	34.5	0.898
	Male	4	13.92 $\pm$ 7.83		
L3 R	Female	18	10.7 $\pm$ 5.12	14.5	0.067
	Male	4	5.5 $\pm$ 2.74		
L3 L	Female	18	10.21 $\pm$ 5.04	16	0.089
	Male	4	5.8 $\pm$ 3.87		
L2 R	Female	18	9.91 $\pm$ 4.17	31	0.67
	Male	4	8.32 $\pm$ 6.2		
L2 L	Female	18	8.92 $\pm$ 3.7	32	0.733
	Male	4	8.35 $\pm$ 5.63		
L1 R	Female	18	11.57 $\pm$ 4.55	27	0.443
	Male	4	8.9 $\pm$ 4.9		
L1 L	Female	18	11.47 $\pm$ 4.93	22	0.233
	Male	4	7.67 $\pm$ 5.04		

SD: standard deviation, U: The Mann-Whitney U value, L: lumbar vertebra, R: right

Table 6. Comparisons of lenke types and mean angle measurements

	Lenke type	n (22)	Mean $\pm$ SD	U	p
L5 R	1	15	16.94 $\pm$ 5.97	45	0.597
	5	7	21.77 $\pm$ 12.6		
L5 L	1	15	18.08 $\pm$ 10.28	52	0.972
	5	7	19.07 $\pm$ 11.25		
L4 R	1	15	12.3 $\pm$ 6.07	51.5	0.944
	5	7	12.74 $\pm$ 4.87		
L4 L	1	15	12.1 $\pm$ 6.06	47.5	0.724
	5	7	13.25 $\pm$ 5.7		
L3 R	1	15	9.78 $\pm$ 5.6	51.5	0.944
	5	7	9.67 $\pm$ 4.42		
L3 L	1	15	9.13 $\pm$ 5.63	45.5	0.622
	5	7	10 $\pm$ 3.93		
L2 R	1	15	9.24 $\pm$ 4.76	44	0.549
	5	7	10.42 $\pm$ 3.97		
L2 L	1	15	8.68 $\pm$ 4.13	49	0.805
	5	7	9.11 $\pm$ 3.84		
L1 R	1	15	11.11 $\pm$ 5.54	51.5	0.944
	5	7	11.04 $\pm$ 1.73		
L1 L	1	15	10.92 $\pm$ 5.74	51	0.916
	5	7	10.48 $\pm$ 3.5		

SD: standard deviation, U: The Mann-Whitney U value, L: lumbar vertebra, R: right

Table 7. Comparison of lenke lumbar modifier and mean angle measurements

	Lenke lumbar modifier	n (22)	Mean $\pm$ SD	U	p
L5 R	A	4	15.07 $\pm$ 5.5	26	0.395
	C	18	19.23 $\pm$ 9.12		
L5 L	A	4	19.7 $\pm$ 19.07	26	0.394
	C	18	18.1 $\pm$ 8.21		
L4 R	A	4	10.725	26.5	0.418
	C	18	12.81 $\pm$ 5.42		
L4 L	A	4	9.55 $\pm$ 6.64	23	0.268
	C	18	13.11 $\pm$ 5.64		
L3 R	A	4	6.46.46	16	0.089
	C	18	10.5 $\pm$ 4.7		
L3 L	A	4	6.77 $\pm$ 8.53	20	0.173
	C	18	10 $\pm$ 4.11		
L2 R	A	4	7.97 $\pm$ 5.5	31	0.67
	C	18	9.98 $\pm$ 4.3		
L2 L	A	4	8.42 $\pm$ 5.51	30	0.609
	C	18	8.91 $\pm$ 3.73		
L1 R	A	4	8.75 $\pm$ 5.76	27.5	0.469
	C	18	11.61 $\pm$ 4.34		
L1 L	A	4	9.35 $\pm$ 6.46	34	0.865
	C	18	11.1 $\pm$ 4.85		

SD: standard deviation, U: The Mann-Whitney U value, L: lumbar vertebra, R: right

less than 5 degrees was found to be 65%. They found that it was 11% in patients with a Δ -angle between 5-15 degrees and 3% in patients with a Δ -angle higher than 15 degrees. Because an open surgical approach was used in our study and we assumed that there would be no force against the superior facet joint,

scenarios that could lead to screw misplacement in the canal were investigated. As the relative angular value decreased, the extent of facet injury in our study appeared to be correlated with the risk of medial breaching.

Table 8. Comparisons of lumbar apex and mean angle measurements

	Lomber apex	n (22)	Mean $\pm$ SD	X ²	p
L5 R	L1	5	26.02 $\pm$ 12.54	3.789	0.285
	L2	7	16.91 $\pm$ 5.03		
	L3	6	16.28 $\pm$ 7.92		
	L4	4	15.07 $\pm$ 5.5		
L5 L	L1	5	22.86 $\pm$ 11.21	2.493	0.477
	L2	7	16.28 $\pm$ 5.19		
	L3	6	16.26 $\pm$ 8.06		
	L4	4	19.7 $\pm$ 19.07		
L4 R	L1	5	14.34 $\pm$ 4.95	0.925	0.819
	L2	7	11.97 $\pm$ 4.72		
	L3	6	12.53 $\pm$ 7.09		
	L4	4	10.72 $\pm$ 6.97		
L4 L	L1	5	14.78 $\pm$ 6.04	1.983	0.576
	L2	7	12.21 $\pm$ 3.68		
	L3	6	12.76 $\pm$ 7.67		
	L4	4	9.55 $\pm$ 6.64		
L3 R	L1	5	10.94 $\pm$ 4.72	5.004	0.172
	L2	7	8.21 $\pm$ 3.95		
	L3	6	12.78 $\pm$ 4.98		
	L4	4	6.4 $\pm$ 6.46		
L3 L	L1	5	10.92 $\pm$ 4.35	3.41	0.333
	L2	7	8.28 $\pm$ 3.86		
	L3	6	11.21 $\pm$ 4.21		
	L4	4	6.77 $\pm$ 8.54		
L2 R	L1	5	10.54 $\pm$ 4.85	0.281	0.964
	L2	7	10.27 $\pm$ 5.08		
	L3	6	9.2 $\pm$ 3.44		
	L4	4	7.97 $\pm$ 5.5		
L2 L	L1	5	9.26 $\pm$ 4.64	1.732	0.63
	L2	7	9.74 $\pm$ 4.06		
	L3	6	7.65 $\pm$ 2.7		
	L4	4	8.42 $\pm$ 5.51		
L1 R	L1	5	10.54 $\pm$ 1.75	1.376	0.711
	L2	7	12.17 $\pm$ 5.45		
	L3	6	11.85 $\pm$ 4.94		
	L4	4	8.75 $\pm$ 5.76		
L1 L	L1	5	9.4 $\pm$ 3.47	0.706	0.872
	L2	7	12.31 $\pm$ 6.1		
	L3	6	11.1 $\pm$ 4.6		
	L4	4	9.35 $\pm$ 6.46		

X²: chi-square, SD: standard deviation, L: lumbar vertebra, R: right

Table 9. Relational analysis of angle measurements

		L1 L	L1 R	L2 L	L2 R	L3 L	L3 R	L4 L	L4 R	L5 L	L5 R
L1 L	r	1.000	-	-	-	-	-	-	-	-	-
	p	-	-	-	-	-	-	-	-	-	-
L1 R	r	0.878**	1.000	-	-	-	-	-	-	-	-
	p	0.000	-	-	-	-	-	-	-	-	-
L2 L	r	0.511*	0.499*	1.000	-	-	-	-	-	-	-
	p	0.015	0.018	-	-	-	-	-	-	-	-
L2 R	r	0.609**	0.625**	0.909**	1.000	-	-	-	-	-	-
	p	0.003	0.002	0.000	-	-	-	-	-	-	-
L3 L	r	0.394	0.380	0.398	0.379	1.000	-	-	-	-	-
	p	0.069	0.081	0.066	0.082	-	-	-	-	-	-
L3 R	r	0.448*	0.494*	0.367	0.411	0.946**	1.000	-	-	-	-
	p	0.037	0.019	0.093	0.058	0.000	-	-	-	-	-
L4 L	r	0.185	0.227	0.333	0.343	0.565**	0.553**	1.000	-	-	-
	p	0.409	0.310	0.130	0.118	0.006	0.008	-	-	-	-
L4 R	r	0.169	0.230	0.189	0.224	0.500*	0.524*	0.897**	1.000	-	-
	p	0.451	0.304	0.399	0.317	0.018	0.012	0.000	-	-	-
L5 L	r	0.265	0.361	0.459*	0.373	0.525*	0.567**	0.728**	0.592**	1.000	-
	p	0.232	0.099	0.031	0.087	0.012	0.006	0.000	0.004	-	-
L5 R	r	0.325	0.419	0.518*	0.487*	0.517*	0.565**	0.711**	0.646**	0.931**	1.000
	p	0.140	0.052	0.014	0.021	0.014	0.006	0.000	0.001	0.000	-

*Significant at the $p < 0.05$ level, **Significant at the $p < 0.001$ level. L: lumbar vertebra, R: right

There are numerous studies in the literature on superior facet injury after pedicle screw placement (11-13). The aim of these studies was to increase surgical safety by revealing the risk factors influencing screw placement in the correct position. In this regard, Cong et al. (12) found that the use of an intraoperative navigation system was an important factor in preventing pedicle malposition. Because of the high cost of navigation systems and the fact that they cannot be used in every spine surgery clinic, special attention should be paid to the factors such as the use of fluoroscopy, printing of 3D spine models, neuromonitoring to increase reliability, and sensitive attention to anatomic markers during freehand techniques (14-16).

Facet tropism describes the presence of asymmetric angles on both sides of the facet joints and is common in various pathologies of the lumbar spine (17). In our study, we found that there was no statistical difference in the angle between the facet and pedicle trajectories on the right and left sides at each spinal level, except for the L5 vertebra in the 3 patients with sacralization. This finding suggests that there is no facet tropism in the scoliotic spine, unless there is some other anatomic variation. Can et al. (18) also found a possible link between facet tropism and sacralization, as observed in our study.

Study Limitations

One of the strengths of the study was the 3D evaluation of tomographic sections via reformat studies, so that the study came

closest to real anatomy (6). Because most studies in the literature use tomographic images without reformatting them to a focused true plane, it is possible that the anatomy will be evaluated in an incomplete plane due to the natural lordosis of the lumbar spine. The weakness of our study was that the patients were not evaluated for postoperative pedicle screw applications. We have two explanations for this. First, screw implantation was not performed at all levels of the lumbar spine (especially at L4 and L5) in patients with AIS, and second, we did not yet implement this method, which we examined in our study, sufficiently in our routine practice to test its effectiveness.

According to our results, the conclusion that "screw insertion with more lateral alignment than facet joint inclination is reliable" applies only to the transpedicular SF screw technique method. In this technique, the midpoint of the anterior cortex of the vertebral body of the screw tip is targeted through the junction of the entry point and the midpoint of the pedicle. In cases where the anatomical methodology is different, such as the cortical bone trajectory technique, this conclusion will not be valid (19).

In the statistical analysis, we could not find a practical margin of safety for any level as a general rule for the placement of pedicle screws. Each patient should be evaluated on his/her own merits in this regard. However, a screw inserted at an angle no more medial than the facet joint, has a higher probability of being in the correct trajectory. Careful review of radiographic images should be

performed in each individual patient prior to surgical intervention when considering the angular inclination of the facet.

CONCLUSION

When implanting a transpedicular screw to correct a scoliotic deformity, a trajectory that is no more medially inclined than the inclination of the facet joint in the axial plane will reduce undesirable events such as medial breaching. This information can be used as supporting information in addition to other anatomical landmarks in pedicle screw applications.

Ethics Committee Approval: The study protocol was approved by the Ethics Committee of Başakşehir Çam and Sakura City Hospital (decision no: 2022.04.102).

Informed Consent: Informed consent was not needed given the nature of the study.

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